

RESEARCH ARTICLE

Fragility of foot process morphology in kidney podocytes arises from chaotic spatial propagation of cytoskeletal instability

Cibele V. Falkenberg^{1☯✉}, Evren U. Azeloglu^{2☯}, Mark Stothers³, Thomas J. Deerinck⁴, Yibang Chen², John C. He², Mark H. Ellisman⁴, James C. Hone³, Ravi Iyengar², Leslie M. Loew^{1*}

1 R. D. Berlin Center for Cell Analysis & Modeling, U. Connecticut School of Medicine, Farmington, CT, United States of America, **2** Department of Pharmacological Sciences, and Division of Nephrology, Icahn School of Medicine at Mount Sinai, New York, NY, United States of America, **3** Department of Mechanical Engineering, Columbia University, New York, NY, United States of America, **4** National Center for Microscopy and Imaging Research, UCSD, San Diego, CA, United States of America

☯ These authors contributed equally to this work.

✉ Current address: Mechanical Engineering Department, Auburn University, Auburn, AL, United States of America

* les@volt.uhc.edu



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Data Availability Statement: All relevant data are within the paper and its Supporting Information files. The spatial model including all equations, geometries and simulations results, are accessible as a public model through the Virtual Cell data base (VCell.org). Segmented and reconstructed SBEM imaging data can be obtained through Dryad data repository at doi: [10.5061/dryad.09d0k](https://doi.org/10.5061/dryad.09d0k)

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Abstract

Kidney podocytes' function depends on fingerlike projections (foot processes) that interdigitate with those from neighboring cells to form the glomerular filtration barrier. The integrity of the barrier depends on spatial control of dynamics of actin cytoskeleton in the foot processes. We determined how imbalances in regulation of actin cytoskeletal dynamics could result in pathological morphology. We obtained 3-D electron microscopy images of podocytes and used quantitative features to build dynamical models to investigate how regulation of actin dynamics within foot processes controls local morphology. We find that imbalances in regulation of actin bundling lead to chaotic spatial patterns that could impair the foot process morphology. Simulation results are consistent with experimental observations for cytoskeletal reconfiguration through dysregulated RhoA or Rac1, and they predict compensatory mechanisms for biochemical stability. We conclude that podocyte morphology, optimized for filtration, is intrinsically fragile, whereby local transient biochemical imbalances may lead to permanent morphological changes associated with pathophysiology.

Author summary

Podocytes are specialized kidney cells with intricate geometries. Regulation of cell morphology and cell-cell interactions is crucial for podocyte function within the delicate glomerular filtration unit. While the cellular cytoskeleton is dynamic, it must be tightly regulated so that the cell shape and the glomerular filter are maintained. However, genetic defects, disease or drugs may perturb the balance of the cytoskeleton regulators or produce local pressure fluctuations causing proteinuria or focal morphological defects. We derived podocyte morphology from 3-D electron microscopy and constructed a mathematical model to study the actin cytoskeleton. The model reveals the potential for local

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chaotic cytoskeletal instability when cytoskeleton regulators (Rac1 and RhoA) are imbalanced. We also explore compensatory mechanisms for pathophysiological imbalances in molecular activities.

Introduction

Podocytes, visceral epithelial cells of the kidney glomerulus, enable the selectivity of the glomerular filtration barrier through their specialized morphology. The cytoskeleton of each highly differentiated podocyte is composed of F-actin, microtubules, and intermediate filaments. All three of these cytoskeletal polymers form the cell body and primary processes, but only actin shapes the foot processes (FPs), the delicate fingerlike projections that interdigitate to form the glomerular filtration barrier [1]. Actin is organized in a spatially specified fashion. Polymerization beneath the plasma membrane gives rise to a cortical actin network, and addition of crosslinkers result in the high density longitudinally aligned bundles, found in the center of the FPs [2]. The FPs establish contact between podocytes and the glomerular basement membrane, in addition to the cell-cell contact via specialized transmembrane junctions called the slit diaphragm, where plasma is filtered [3]. As a result of their highly dynamic filtration function, each FP must withstand tensile stresses (due to glomerular expansion during systole) and transverse shear stresses (imposed by the fluid flow crossing the slit diaphragm), while maintaining contact with the neighboring cells as well as the basement membrane [4, 5]. The loss of the characteristic FP morphology (i.e., foot process effacement) and reduction in the number of podocytes are common hallmarks of chronic kidney disease (CKD), whereby glomerular filtration becomes compromised and protein appears in urine (i.e., proteinuria) [6, 7]. The limited treatment options for CKD are in part due to the sensitive nature of these highly differentiated cells.

Podocytes rapidly dedifferentiate after isolation of glomeruli, losing expression of key slit diaphragm proteins and the specialized morphology within 8 hours, and fully reverting to amorphous epithelial cell morphology within 48 hours [8]. Cultured primary or immortalized podocytes fail to fully differentiate [9]. These observations suggest that the mechanical stresses experienced by the podocyte in the mammalian glomerulus may regulate the integrity of the actin cytoskeleton within the FPs. Without the *in vivo* mechanical stimuli and the final shape signals, cultured podocytes present geometric characteristics (e.g., surface-to-volume ratio, eccentricity, characteristic length, etc.) that are clearly different from the *in vivo* structure [10, 11]. Consequently protein localization, gene expression levels, and active signaling pathways in cultured podocytes are not similar those of the *in vivo* cells [12]. Slit diaphragm has not yet been reconstituted in culture; hence, the unique localization of podocyte specific proteins that lead to the pro-differentiation signaling landscape and the stable actin cytoskeleton of the FPs is absent in cultured podocytes *in vitro* [13, 14]. To understand how the maintenance of the FP morphology and slit diaphragm integrity are regulated, it is important to study the balance of signals within the context of the *in vivo* cell morphology.

Rho GTPases play important roles in the regulation of the actin cytoskeleton [15]. Rac1 promotes the formation of a branched actin network, as found in lamellipodia whereas, RhoA promotes the formation of stress fibers and actin bundles. Expression and activity of both of these GTPases are tightly regulated in the healthy podocyte [16]. For example, while Rac1 knockdown may prevent protamine sulfate-driven FP effacement (a standard animal model of acute podocyte injury), suggesting increased FP stability, Rac1 knockout animals that are subjected to chronic hypertension exhibit FP loss, proteinuria and glomerulosclerosis, showing an

opposite effect [17]. Proteinuria and focal FP effacement are also observed when Rac1 is hyperactive [18]. It is not clear how an actin polymerization signaling hub, such as Rac1, may act both as a stabilizing and destabilizing factor under these varying mechanical conditions. It is also puzzling that similar phenotypes could be observed for both Rac1 knockdown and overexpression. A similar outcome is observed with RhoA activity. *In vivo* induction of constitutively active or inactive RhoA damages the actin cytoskeleton causing loss of foot processes and proteinuria [19, 20]. These findings indicate that the levels and activities of both RhoA and Rac1 need to be within a defined range to maintain morphological integrity of the foot processes. What is the quantitative relationship between local morphology and the GTPase regulators of biochemical and biophysical reactions underlying actin cytoskeleton dynamics that stabilize podocyte FPs? To answer this question, we need to develop computationally tractable models based on realistic *in situ* morphologies. We developed dynamical models that combine upstream GTPase signaling with mechanical forces that control the podocyte actin cytoskeleton. Our models account for the actin stoichiometry, exchange between monomeric, filamentous, or bundled states, and the *in vivo* podocyte morphology. To account for the spatial specificity of the complex 3-D geometry of the FPs *in vivo*, we constructed a new quantitative model of a representative podocyte using 3-D serial blockface scanning electron microscope (SBEM) imaging in healthy rats. Our 3-D reconstructed model has sufficient resolution to capture the relationship between volume, surface area and characteristic length of the podocyte geometric features as well as the underlying biochemical and biophysical reactions. Our cytoskeleton model and the spatially specific simulations provide a mechanistic understanding of the *in vivo* observations regarding Rac1 and RhoA dynamics in podocytes, and their relationship to the cytoskeletal stability of FPs. The spatial simulations reveal the emergence of chaotic spatial heterogeneities within the actin cytoskeleton when Rac1/RhoA balance is altered providing a multiscale mechanism for foot process effacement due to propagation of chaotic behavior across FPs. Using this dynamical model, we also show how compensatory mechanisms could impact podocyte cytoskeletal integrity when they appear at different stages of regulatory dynamics.

Results

Podocyte morphology

We reconstructed the *in situ* 3-D geometry of interacting podocytes that would represent core spatial features of a podocyte that permits spatial modeling. SBEM image stacks were processed by manual segmentation and Gaussian filtering to reconstruct podocyte geometry with arborized processes that included nanoscale cell-cell junctions at the foot processes (Fig 1, Supplementary S1 Video). These reconstructions revealed a complex configuration of primary branches emanating from the cell body (Supplementary Material 1). Branching angles and the extent of secondary branching for these processes varied; however, the length and number of processes were similar among different podocytes (S1 Fig); also, despite the large level of deviations in the shape and projection pattern for primary processes, other key geometric characteristics, such as volume, principal dimensions, and surface area of individual podocytes exhibited remarkably low variability between individual podocytes (Table 1). While these studies were in progress, another report used SBEM to reconstruct qualitative features of podocytes [21]. Our reconstruction focused on identifying quantitative spatial parameters that could be used in dynamical models. The results from the analysis of five healthy rat podocytes are summarized in Table 1, with the steps required to achieve this analysis illustrated in Fig 1A–1D.

We assigned quantitative geometric parameters for podocyte morphology into three distinct compartments based on their reaction-diffusion dynamics: cell body (CB), major

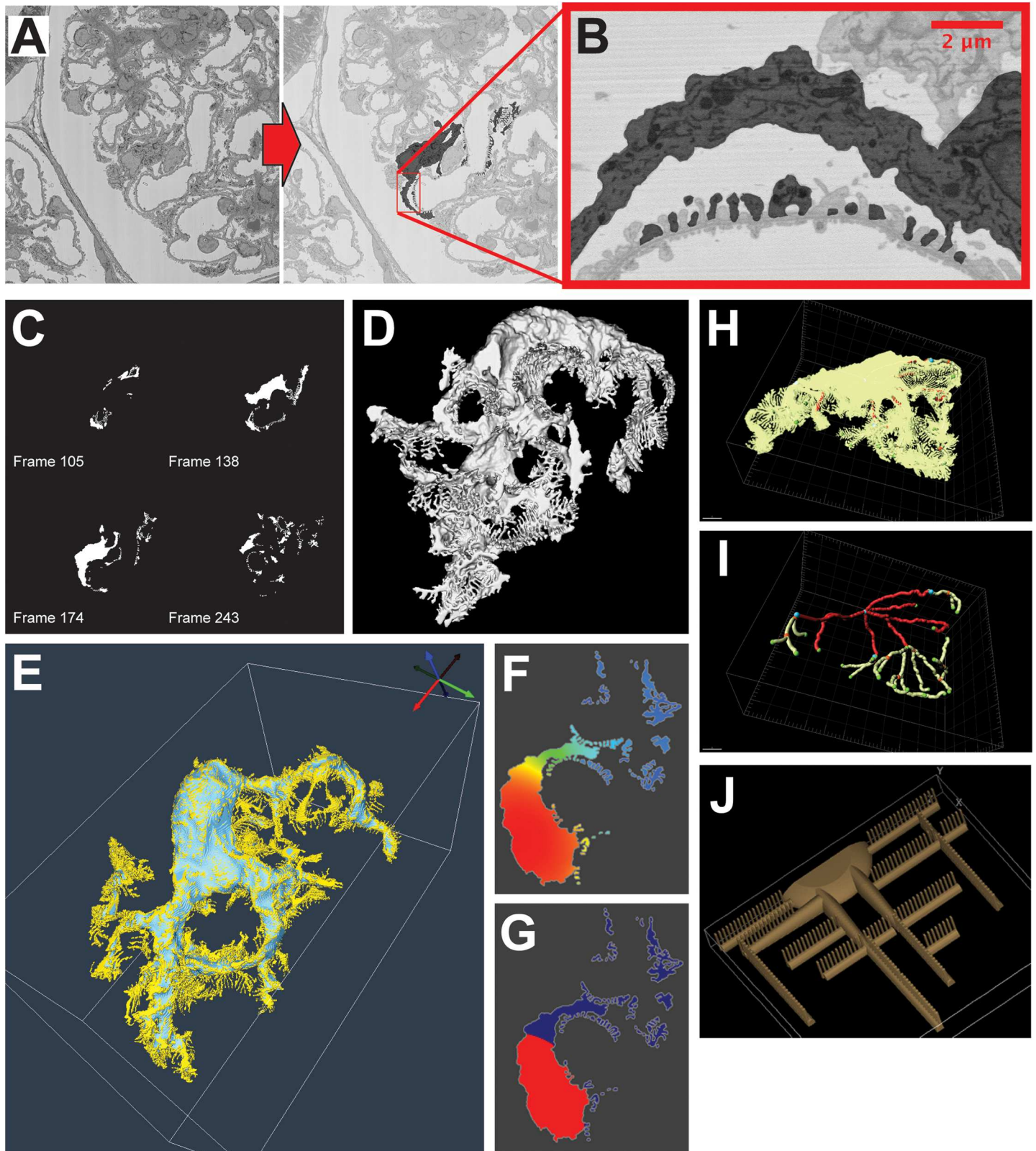


Fig 1. Image segmentation, volume reconstruction, and quantitative analysis of podocyte morphology. (A) In order to reconstruct the complete podocyte volume including all the foot processes, we manually segmented stacks of SBEM images. This was done by reviewing the entire stack and

identifying all of the projections that emanate from the cell body. **(B)** At full resolution, geometric details of individual foot processes can be seen. **(C)** We then thresholded the segmented images to obtain continuous binary stacks that can be extruded in Rhinoceros and combined in Virtual Cell to form **(D)** a reconstructed 3-D volume. **(E)** We quantified the volume and surface area share of foot processes (FPs) by imposing a Gaussian surface filter in Seg3D, which removed all surface projections smaller than 440 nm. **(F)** We used a commonly used heat transfer model to identify the cell body of the cells: a cytoplasmic specie was uniformly synthesized and allowed to diffuse into the membrane until steady state. Regions with low surface area-to-volume ratios, i.e., cell body, maintain ~90% of the maximum value. **(G)** These sections were assigned as the cell body. **(H)** From the reconstructed volumes, length and angles for major processes and branches were measured using Imaris; the lime colored rendered volume represents the cell volume whereas colored internal lines are the measured paths for the branches. **(I)** For clarity, the internal lines are shown without the rendered volume. Sample branching patterns for two of the cells are shown in supplementary S1 Fig. **(J)** Using the volume, surface area, and branching information, a representative geometry is constructed. For computational simplicity, we assumed symmetry about the xy- and yz-planes, and hereby only half of these are shown. Rat podocytes (RP) used in this figure are RP1, RP8, RP9, RP11, and RP13, respectively, and morphological characteristics of these cells are shown in Table 1.

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processes (MP) that includes primary and secondary processes, and FPs, denoted with appropriate subscripts, respectively. We also reconstructed the nucleus (Nu) although it was not used in the dynamical models. The volume, *V*, and surface area, *A*, without subscripts, represent the respective parameters for the whole cell. The CB, MP and FP volumes were derived from the segmented images. Different filters that were based on reaction-diffusion dynamics, allowed reconstruction of a whole cell (yellow surface in Fig 1E) and a “foot process-free cell” (blue surface in Fig 1E). The volumetric properties were computed using Seg3D (Center for Integrative Biomedical Computing at University of Utah, Salt Lake City, Utah, USA) and Virtual Cell (Center for Cell Analysis and Modeling at University of Connecticut, Farmington, CT, USA) (Supplementary Material 1). Boundaries of the different spatial components of the cell were estimated by applying a stratification method that is analogous to a well-known heat transfer problem [22]. The primary processes of a podocyte have a large surface-to-volume ratio in comparison to its cell body. Therefore, a podocyte with uniform volumetric synthesis and diffusion of a given protein within its entire volume and with transport of protein to the extracellular space (proportional to local intracellular concentration) will equilibrate to a much lower concentration at the primary processes relative to the cell body (Fig 1F and 1G, analog heat transfer problem of uniform heat generation with convective boundary condition).

Our analysis revealed that the CB volumes range from 30 to 50% of the total cell volume. FPs correspond to 20% of the total cell volume but constituted nearly 60% of the surface area; the remaining 50% to 30% of the volume corresponds to MP. The distances between the center of the CB and branch points, or ends of the MP, were measured using the filament tool in Imaris (Bitplane, Zurich, Switzerland), as shown in Fig 1H and 1I.

Table 1. Geometric properties, such as surface area (A) and volume (V), of healthy adult rat podocytes are categorized according to different segments of the cell, namely: cell body (CB), major processes (MP), and foot processes (FP) of each rat podocyte (RP). The last column outlines the quantitative morphometric parameters used to generate the idealized, representative podocyte geometry.

Cell	RP1	RP8	RP9	RP11	RP13	Mean	St. D.	Idealized
$A_{Co+MP} / V_{Co+MP}, \mu^{-1}$	1.8	1.9	1.9	1.5	1.5	1.7	0.2	1.7
$A / V, \mu m^{-1}$	3.2	3.2	3.4	2.6	3.0	3.1	0.3	3.2
$A_{FP} / V_{FP}, \mu m^{-1}$	8.2	8.6	8.8	8.4	9.3	8.7	0.4	9.0
$(A - A_{CB+MP}) / A_{CB+MP}, \%$	130	110	130	100	150	120	20	140
$V_{FP} / V, \%$	22	19	21	16	20	20	2	20
No of branches	43	30	34	31	34	34.4	5.1	36
Length of branches	10.5	10.4	12.0	11.2	10.7	11.0	0.7	-
$V_{CB} / V, \%$	38	33	21	46	50	38	11	-
$V_{MP} / V, \%$	40	47	57	38	31	43	10	-
$V_{Nu} / V_{CB}, \%$	24	42	42	24	22	31	10	-

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Since the branching parameters such as process length, counts, and distances were widely variable, we utilized the analytical descriptors of segregated volumetric units to construct a representative podocyte. From this analytical geometry, we obtained relevant reaction-diffusion equation parameters (length, surface area, and volume) at the whole cell level. The application of symmetry allowed us to reduce the mesh sizes needed for numerical discretization and the computational cost. FPs emanate from major processes in a symmetrical fashion. Therefore, in our analytical geometry, the major processes are generated as halves, using the sagittal plane as a reflexive boundary condition. The FPs emanate perpendicularly to such a boundary. Since there was no signature branching pattern for these cells, we also imposed axial symmetry. Consequently, the analytically constructed geometry produces simulations of a full podocyte cell, but at a quarter the size (Fig 1J).

The representative geometry was initially built by taking into account only the cell body and major processes. Once the surface-to-volume (see Table 1) and distances of $18 \pm 6 \mu\text{m}$ average distance from centroid to branch point, and $39 \pm 2 \mu\text{m}$ for the three furthest endpoints, satisfied the analysis described above, the FPs were added. The quarter of the cell (CB plus MP) had a volume of $420 \mu\text{m}^3$ and surface area $695 \mu\text{m}^2$. After 233 FPs were added, the final volume was $530 \mu\text{m}^3$ and surface area was $1683 \mu\text{m}^2$ (Fig 1J). Table 1 demonstrates that the volumetric properties of the constructed geometry correspond to a good representation of the analyzed experimentally imaged cells. The surface area of the constructed FPs is on the upper range of the analyzed values. This is likely a conservative estimate; the resolution of the acquired images is of the length scale of the FPs, and a loss of surface detail is expected. The non-spatial computational model described below only uses volumetric variables, and is not affected by this assumption.

Actin cytoskeleton dynamics in the foot processes

To allow us to understand how actin cytoskeletal dynamics must be regulated to maintain this extraordinary cellular structure, we built a minimal kinetic dynamical model that describes the exchange of actin between monomeric (G-actin), filamentous (F-actin) and bundled states. While the model vastly reduces the complexity of the actual biochemical machinery underlying actin dynamics [23–25], the equations and parameters are approximately related to the key mechanisms controlling polymerization and bundling. For example, a generic “bundling coefficient” is used rather than different expressions corresponding to individual molecular contributors of actin-associated proteins or crosslinkers for bundling. However, different parameters in the model can be related to the activity of Rac1 and RhoA, allowing us to use these as surrogates for the corresponding signaling pathways. Based on experimental observations [26], the actin cytoskeleton in the FP maintains its morphological stability. We used this cytoskeletal model to determine how the balance of GTPase activity affects the spatial stability of FP actin cytoskeleton and consequently its morphology. Initially, we developed an ordinary differential equation (ODE) model. We then mapped the ODE model to the reconstructed podocyte geometry and solved the reaction-diffusion equations for the corresponding partial differential equations (PDEs) numerically.

Fig 2A shows the relationship between each state and the nomenclature used for parameters. We focused on the three discrete states of the actin cytoskeleton: namely monomeric G-actin, filamentous F-actin, and bundles (i.e. stress fibers), represented by the variables G_a , F_a , and B_u , respectively. The model is described by Eqs 1–3. In Eq 1, the parameter γ_f lumps polymer elongation activity ($\gamma_f^* G_a^* F_a$) and nucleation activity ($2^* \gamma_f^* G_a^* G_a$), as both will produce F_a ; for nucleation, the coefficient is necessary for mass conservation since dimerization will form a filament containing 2 actins. The assumption that γ_f can represent both elongation and

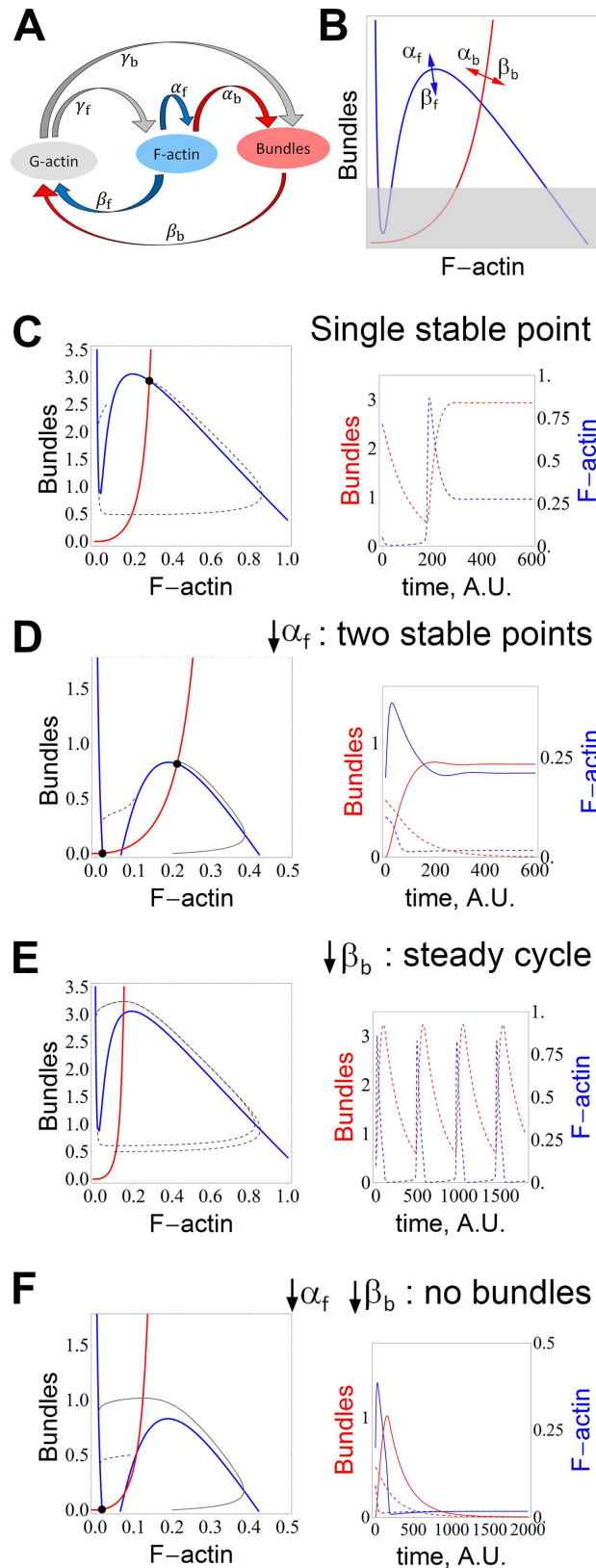


Fig 2. Minimal kinetic model for actin cytoskeleton in FPs. (A) Reaction diagram and nomenclature for parameters. Each parameter represents the rate of conversion between the two species marked by the

arrows. **(B)** Summary for relationship between nullclines and parameters α_f , β_f , α_b and β_b . Blue curves are nullclines for Eq 1 and red curves for Eq 2. The arrows represent the direction of change of a given nullcline when the shown parameter increases. The gray shaded region represents the “effacement region” where actin in FPs does not form adequate amount of bundles and maintain a stable FP morphology. **(C)** A system with strong positive feedback (α_f , or weak dissociation rate, β_f) has a single stable equilibrium point. The concentrations for bundles and F-actin in the dashed trajectory of the phase plane (left, dashed gray line) are plotted in the time-series to the right, in red and blue, respectively. **(D)** Weak positive feedback (α_f) or strong dissociation rate (β_f) give rise to a second stable equilibrium point, representing the collapse of bundles. The concentrations for the solid trajectory in the phase plane (left) are plotted with the solid lines in the time series (right). **(E)** Weak bundle turnover rate (β_b) or strong bundling (α_b) destabilizes the system, and there are no longer stable equilibrium points. However, the cyclic behavior might be able to keep the bundles sufficiently strong at all times. **(F)** A combination of weak bundle turnover rate (β_b or strong bundling, α_b) and weak positive feedback (α_f) results in complete collapse of the actin cytoskeleton. Model parameters listed in S1 Table. All concentrations are non-dimensional.

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nucleation does not impact the model analysis, as presented in greater detail in the supplementary material (S2 and S3 Figs). The filament state is further enhanced by positive feedback in the first term on the right hand side of Eq 1, which describes nucleation mechanisms that depend on pre-existing filaments, such as Arp2/3-dependent branched nucleation. This term lumps the polymerization triggered by phosphorylation of nephrin and focal adhesion signaling through Nck, N-WASp or Rac1 [27, 28], and represented by a Hill function. Increasing the Hill coefficient does not change the qualitative behavior of the system (S3 Fig). Therefore the parameter α_f is non-zero only within the volume representing FPs, where nephrin signaling is localized. A non-linear functional form is necessary to represent both nephrin and small GTPase Rac1 driven polymerization [29–31]. The denominator identifies the high sensitivity region (the positive feedback term is only significant if Fa is at least of the same order of magnitude as the parameter k), and ensures that the effective rate constant is bounded.

In Eq 2, activation of RhoA and crosslinking factors result in the formation of actin bundles. In the first term on the right hand of Eq 2, new bundles are formed by merging filaments while existing bundles grow by addition of filaments, both governed by α_b . Actin monomers can also be added to filaments within bundles ($\gamma_b * Ga * Bu$). Once a filament becomes bundled, more crosslinks are added and it is unlikely to simultaneously break all connectors between a single filament and the bundle it belongs to. However, there is dissociation of monomers either from depolymerization or biomechanical stress-related rupture, both for filaments and bundles; we represent these, respectively, as $-\beta_f * Fa$ and $-\beta_b * Bu$ [32, 33] in Eqs 1 and 2, respectively. Eq 3 describes mass conservation within the cell. There are filaments and bundles in all parts of the cell; but we assume that the Ga pool is not strongly affected by dynamics of turnover of the F-actin in the CB and MP, and that crosslinked actin bundles are strongly localized to the FPs [26]. Therefore, we concern ourselves with the FP actin dynamics, where the small volume may lead to large changes in Fa or Bu. Thus, we consider the species Fa and Bu only within the FPs, while Ga freely diffuses to the different regions of the cell, as indicated by the different volume domains for the integrals in the mass conservation equation.

$$\frac{d(Fa)}{dt} = \alpha_f Ga \left(\frac{Fa^2}{Fa^2 + k^2} \right) + \gamma_f Ga (Fa + 2 Ga) - \alpha_b Fa (2 Fa + Bu) - \beta_f Fa \quad (1)$$

$$\frac{d(Bu)}{dt} = \alpha_b Fa (2 Fa + Bu) + \gamma_b Ga Bu - \beta_b Bu \quad (2)$$

$$\text{Total actin} = \int_{cell} Ga dV + \int_{FP} Fa dV + \int_{FP} Bu dV \quad (3)$$

Since the exact concentrations of actin at each state in the podocyte are unknown, all of the concentrations in the above equations are set as non-dimensional entities, which would allow quantitative comparison of state spaces. It is known that the ratio of total amount of monomeric actin to polymerized actin in the healthy podocyte is about 1:2 [34]. Here, we use the term “bundle concentration” to represent the concentration of actin molecules in the cross-linked bundle state.

The intersections between the nullclines (lines identifying values of variables that result in zero time derivative) for the variables F-actin and bundles reveal the equilibrium points for the system; increasing any of the parameters presented in Fig 2B will move each nullcline as indicated by the arrows (also in S4 Fig). Bundles are able to sustain mechanical stress better than a filamentous network, and a minimum bundle density is expected to be necessary for the morphological integrity of the individual FP [35]. If the polymerization or bundling rates are not sufficient to overcome the turnover rates, the equilibrium point moves to the “effacement region” of the diagram that is demarcated with gray shading, where loss of FP integrity and specialized morphology (i.e., effacement) is expected.

The behavior of the non-spatial ODE model reconciles the varied experimental findings on the roles of Rac1 and RhoA

As illustrated by the two trajectories in Fig 2C, under conditions of a parameter regime with a single stable point, the FPs are able to sustain strong bundles irrespective of the initial conditions, or perturbation. This diagram represents ideal circumstances for a healthy stable podocyte. In contrast, reduced filament formation (due to decreased Rac1 activity, or defective Nck signaling) creates a second stable equilibrium point (Fig 2D). If the system moves to this new state, with negligible bundles, the FP morphological integrity will be lost (since this point is located in the effacement region of Fig 2B). Another parametric set that may result in destabilization of the system and loss of FP morphological integrity is via increased bundling (α_b) or decrease in the turnover of the bundles (β_b). Depending whether α_f is high or low, it may be subject to a cyclic behavior or collapse, respectively (Fig 2E and 2F). The results in Fig 2 correspond to a non-spatial model of actin dynamics, with FPs comprising 20% of the total volume (Eqs 1–3).

The behaviors described by the model are consistent with the experimental observations for response to different activity levels of RhoA *in vivo*. A basal level of RhoA in podocytes (known to activate myosin and promote bundling) has been shown to be necessary for healthy glomerular function [20]. Weak bundling (α_b) would move the equilibrium point towards higher concentration of F-actin and lower concentration of bundles, shifting the equilibrium point towards the effacement region shown in Fig 2B. In the non-spatial model, the reasons for the damage caused by hyperactive RhoA are not obvious. Our model suggests that RhoA hyperactivity may lead to an imbalance between bundling and depolymerization, where the bundles “consume” all the actin, and the minimum density of filaments required for the positive feedback is no longer achieved. Eventually, the filament density becomes too low and the bundle turnover surpasses its formation. Once this happens, the cytoskeleton may either be subject to temporary (Fig 2E) or terminal collapse (Fig 2F). As the bundles collapse, more monomeric actin becomes available. If the positive feedback for filament growth is sufficiently strong, the filament density recovers and the bundle density increases, resulting in cycles of weaker and stronger bundle density. The instances of weaker bundles may be sufficient to make the FP more susceptible to effacement under increased stress or even under physiological conditions. This scenario is further explored by spatial modeling in the next section.

A weaker positive feedback (α_f) is the mathematical representation of a system where Rac1 is inhibited. The low α_f -system in Fig 2D has a stable equilibrium point with moderate

bundles. The presence of another stable point, which represents the collapsed cytoskeleton (minimal bundles or filaments), demonstrates that this region of parameter space is not as robust as the system with a single stable point as shown in Fig 2C. In addition, sustained bio-mechanical stress (e.g., high blood pressure) corresponding to increased β_b in the model, moves the bundle nullcline as indicated in Fig 2B, further decreasing the bundle concentration of the stronger stable point. Our model agrees with the physiological observation that, under such conditions, morphological damage may be observed [17].

Diffusion limited process breaks the oscillatory synchrony, resulting in progressive localized damage

When we use a partial differential equation (PDE)-based dynamical model with the representative 3-D podocyte geometry shown in Fig 1J, we observed spatial heterogeneities in the oscillatory behavior (Fig 3). This gives rise to permanent localized loss of bundles, leading to effacement of FPs (Fig 3A–3D). As monomeric actin is consumed, it must diffuse from its largest pool in the cell body to all FPs. The varying distance from this major G-actin source to the arrays of FPs, which act as individual G-actin sinks, produce gradients in G-actin, triggering asynchronies in the availability of G-actin at individual FPs. Thus, bundles are collapsing in some FPs, while being strengthened in others. Consequently, as some FPs “release” their pool of G-actin, those monomers are sequestered by neighboring FPs, which are reciprocally reinforced. Fig 3B and 3C show the bundle concentration at different times after α_b is increased. After elimination of some FPs, the remaining ones are able to build stronger bundles, temporarily enhancing their ability to overcome stress. However, the system is still unstable and morphological changes would progress slowly. Examination of Fig 3C, in particular, shows that although this is a purely deterministic system, the spatial pattern of bundle loss among the FPs appears to be random. Furthermore, the precise value of the perturbation in α_b will produce different patterns. For example, different α_b will result in a different steady cycle amplitude range and frequency in the ODE model, which will be translated into a different pattern for the loss of synchrony in the spatial model. Such unpredictable behavior following a change in initial conditions is the hallmark of a chaotic system. Fig 3D shows how the asynchrony can be followed by permanent damage in some FPs. In some of the FPs, bundle concentrations drop permanently to 0, this would correspond to FP effacement. This example illustrates the potential impact of hyperactive RhoA on the FP morphological integrity.

Localized or transient Rac1 hyperactivity can damage the podocytes

Each podocyte is subjected to spatially varying mechanical and biochemical signals: it adheres to the basal lamina supporting a segment of the coiled glomerular capillary vessel, and it interacts with several other podocytes. The cell-cell and cell-basement membrane interactions may lead to enhanced Rac1 activity, downstream of transmembrane slit diaphragm protein nephrin or focal adhesions [28, 36]. Using our spatial model, we can demonstrate how this could lead to local damage. The ODE system with parameters as in Fig 2C has a single stable solution. However, this model is only valid if all parameters are uniform among all FPs. To explore and analyze the effect of differential actin bundling activities, we enhanced the ODE model to include two compartments (S2–S6 Eqs). The monomer G_a is assumed to diffuse infinitely fast, resulting in the same concentration in the two compartments. The fraction “FP₁” of the FPs in compartment 1, retain the original value of α_f , while there is a localized increase in the positive feedback strength for the complementary fraction of FPs, “FP₂”, in compartment 2. Fig 4A shows the steady state response for bundle concentrations in such an asymmetric cell, with constant positive feedback values α_f and $\alpha_f + \Delta\alpha_f$ for the fractions of FPs labeled FP₁ (blue

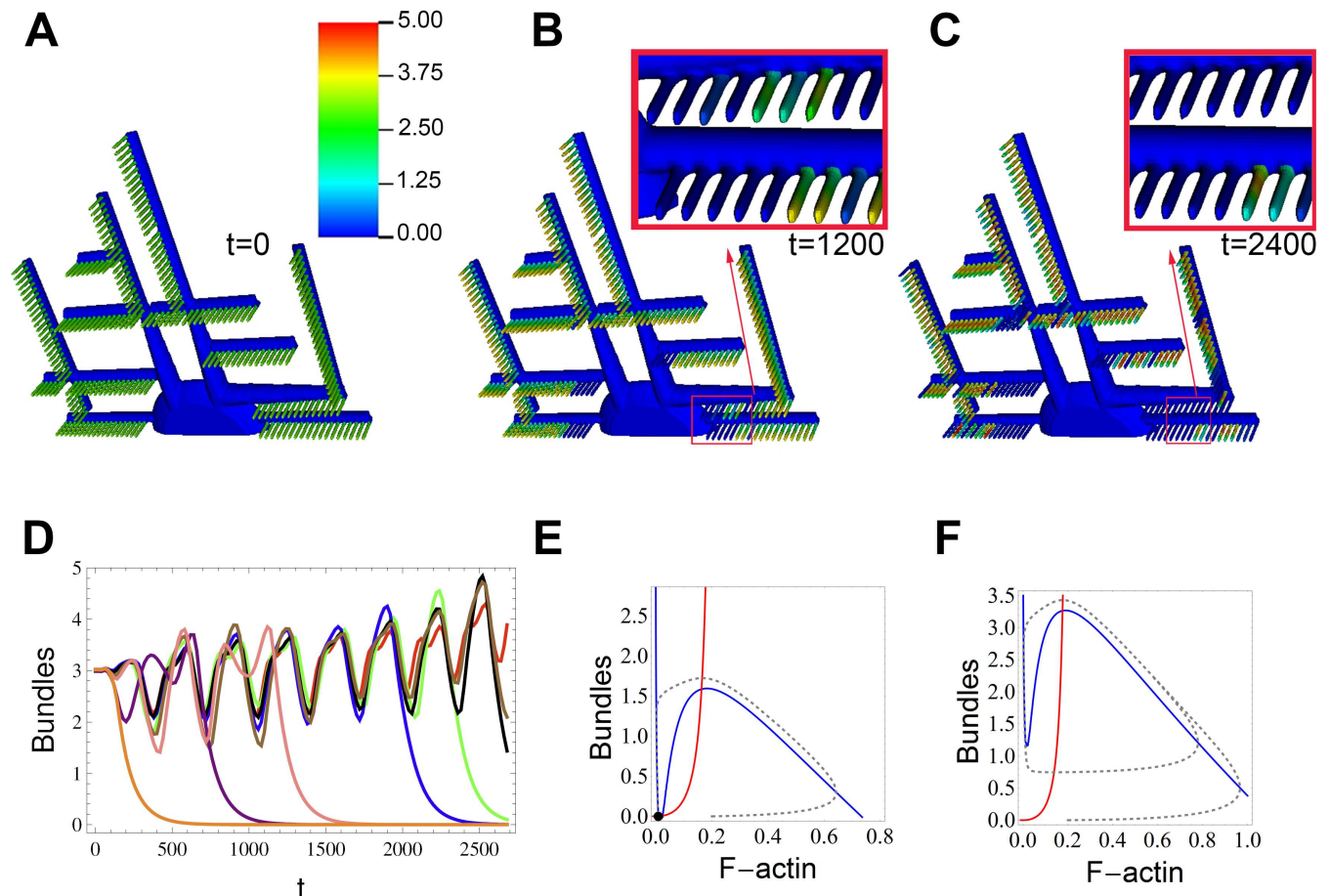


Fig 3. Impact of hyperactive bundling, α_b , on FP actin stability. Spatially, the cyclic behavior (triggered by sudden, but spatially uniform, increase in α_b at $t = 40$) gives rise to asynchronous and progressive loss of actin bundles within FPs (A-D). (A) Spatial steady state actin bundle concentration; simulation parameters are same as those highlighted in Fig 2C. (B) Snapshots of bundle concentration in response to increased bundling, at time $t = 1200$ and (C) time $t = 2400$. Insets correspond to magnified and slightly rotated view of respective boxes. The colorbar represents bundle concentration in normalized arbitrary units. (D) Timecourse of bundle concentration at randomly picked FPs, demonstrating asynchronous collapse of bundles. (E) ODE solution for increase in α_b predicts cytoskeleton collapse when the actin pool is reduced to 70% of that in Fig 2. (F) For systems with larger pools of actin (115%), stronger yet still unstable bundles are predicted. In spatial simulations the positive feedback, α_f , is localized to FPs only, and zero elsewhere.

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mesh) and FP_2 (red mesh), respectively. As expected, for small values of $\Delta\alpha_f$ each fraction of FPs have a new concentration of bundles, weaker (FP_1) or stronger (FP_2) than when $\Delta\alpha_f$ is 0 (green line). As $\Delta\alpha_f$ and FP_2 fraction increases, the bundles in the region FP_1 collapse. Also note that as FP_2 fraction increases, the total amount of actin becomes a limiting factor, and the local strength for the bundles cannot reach the high values observed in small FP_2 fractions. This plot also illustrates that even though the machinery for F-actin polymerization is ubiquitous, the regions of the cell that are able to gather stronger polymerizing factors outcompete the remainder of the cell for the primary resource (G-actin), resulting in uneven distribution of F-actin and bundles. This result is consistent with the observation that in podocytes, regulation of the actin cytoskeleton is tightly controlled in the FPs [26], where a high concentration of proteins that mediate actin polymerization are specifically localized [37].

Fig 4C–4E show the impact of a localized transient enhancement (shown in Fig 4B) of the positive feedback on region FP_2 only (50% of the FPs). If the stimulus is weak, both FP_1 and FP_2 regions recover the uniform bundle strength (blue and red lines, respectively, in Fig 4C).

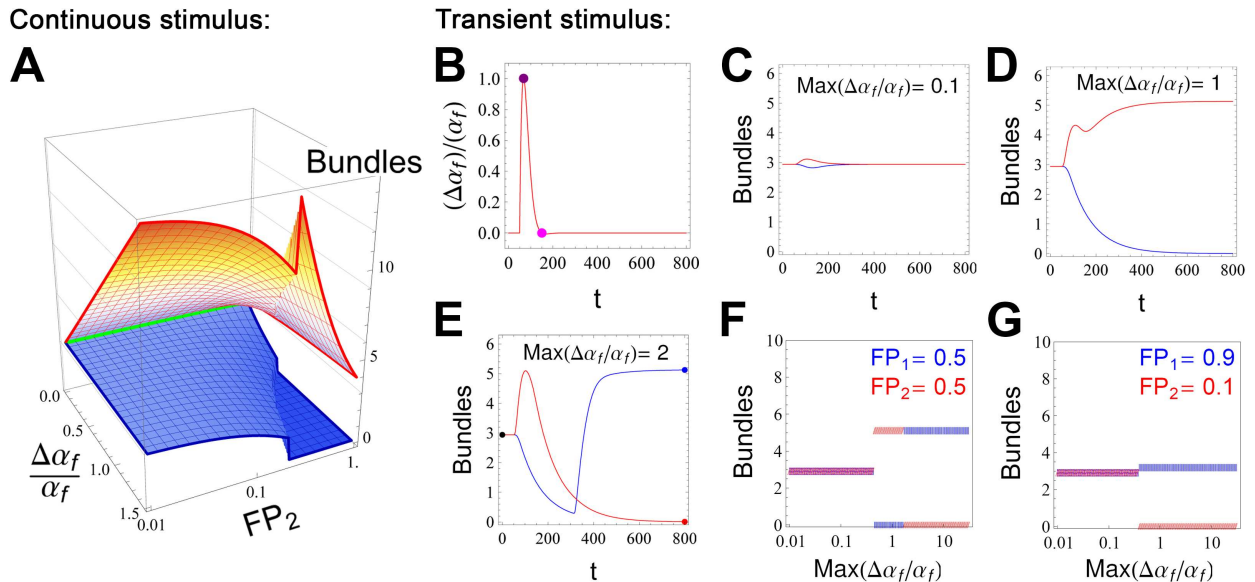


Fig 4. Analysis of bundle stability in the face of spatial differences in positive feedback (α_f), using an ODE model composed of 2 FP compartments. One FP fractional compartment (FP_2) is subject to a stimulus that increases actin polymerization by $\Delta\alpha_f$, whereas the remaining fraction (FP_1) is subject to nominal polymerization conditions, α_f . This stimulus may either be sustained (shown in A) or transient (shown in B-G). (A) A 3-D plot showing steady state bundles on the vertical axis as a function of $\Delta\alpha_f/\alpha_f$ and FP_2 (log scale). For this sustained enhancement, the bundle intensity in FP_1 (blue mesh) and FP_2 (red mesh) depend on the intensity $\Delta\alpha_f$ and the relative proportions of FP_2 to FP_1 ($FP_1 + FP_2 = 1$). As $\Delta\alpha_f$ increases, FPs with stronger feedback form stronger bundles. If the fraction of FPs with enhanced feedback (FP_2 , red mesh) is small, the FPs with normal α_f (FP_1 , blue mesh) are unperturbed, while the bundles in FP_2 are strengthened. Because there is a fixed total amount of actin, stronger bundling in FP_2 drains actin available for bundles in FP_1 until a threshold is reached at which collapse of actin bundles in FP_1 is observed. (B) Time course of a transient stimulus applied at $t = 40$. In C-E, the value of $\Delta\alpha_f$ follows this time course, with varying intensities; equal volume fractions for FP_1 and FP_2 were used, with red curves corresponding to FP_2 and blue to FP_1 . (C) A small perturbation allows the system to return to the pre-stimulus steady state. (D) When the maximum $\Delta\alpha_f/\alpha_f = 1$ (i.e. FP_2 transiently reaches twice that of FP_1), a new stable steady state is generated where bundles have collapsed in FP_1 and increased in FP_2 . (E) When the maximum $\Delta\alpha_f/\alpha_f = 2$ (i.e. FP_2 transiently reaches 3 times that of FP_1) there is a transient increase in FP_2 bundles followed by collapse and enhanced bundles in FP_1 . The behavior displayed in C, D and E is the hallmark of a tristable system. See the text for an explanation. (F). The steady state values for concentration of bundles in fractions FP_1 (blue) and FP_2 (red) are shown as a function of stimulus intensity, consistent with C-E. (G) Different fractions of FP_1 and FP_2 will impact the steady state values (see also S6 Fig).

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For moderate stimulus, FP_1 fraction loses bundles permanently and FP_2 reaches a new steady state, with stronger bundles (Fig 4D). For very strong $\Delta\alpha_f$, the initial response is as expected, but at longer times, the bundles in FP_2 collapse while the bundles in FP_1 are enhanced Fig 4E). The phase-plane diagrams in S5 Fig help explain the switch. At time zero, either FP_1 or FP_2 fraction has the same composition regarding bundles and F-actin. With strong $\Delta\alpha_f$, FP_2 fraction consumes G-actin in order to develop more and more filaments, while the production rate of filaments for FP_1 becomes weaker than its turnover. At this point, the two regions of FPs are asynchronous, and their volume fractions and proportions of F-actin and bundles (i.e., their position in the phase-plane) will determine which fraction “wins over” the available G-actin (note the trajectories in Fig 2C). In summary, the steady state response to a localized transient peak in the polymerization positive feedback can either lead to both regions of the FPs to recover the original uniform bundle concentration, or lead to one of the stimulated (FP_2) or unstimulated (FP_1) regions to collapse (S6 Fig).

The same range of responses was observed in our spatial simulations. Consistent with the results in Fig 4C–4G, the spatial simulations revealed that localized transient increase in the positive feedback α_f may lead to localized changes in bundles, both in the regions within and adjacent to the stimulus (Fig 5). Time zero has all FPs in steady state and at same bundle

concentration (as in Fig 3A). After time 40, only the region FP₂ (as marked in Fig 5) is subject to a transient increase in the parameter for positive feedback α_f , while all other FPs are subject to constant α_f (all the other FPs in highlighted region are FP₁, time series for the feedback parameter α_f is shown in S7 Fig). The timeseries plot in Fig 5A indicates the bundle concentrations in FPs identified by the corresponding colored arrowheads. Because the availability of monomeric actin is diffusion limited, a gradient of responses is observed. Within the region FP₂, there are FPs that recover the original bundle concentration once the stimulus is removed (e.g., the FP indicated by the orange arrow head in Fig 5A). There are also FPs that collapse within the same region (red arrowhead). Interestingly, it is the FPs near the boundary that permanently lose their bundles. Similarly, among the FPs in close proximity to FP₂ (yet with constant α_f), some also permanently collapse (blue arrowhead). The 3-D movie of Fig 5 is in Supplementary S2 Video. In the movie, the bounding box identifies the region FP₂. A second example is shown in Supplementary S3 Video, with a significantly larger region for FP₂, comprising all FPs within the bounding box.

Compensatory mechanisms: The earlier, the better

Next, we studied the impact of decreasing bundle turnover rate β_b and the potential ways to regulate podocyte FP integrity. Bundle turnover rate, β_b , accounts for depolymerization and damage of bundles due to mechanical stress in the glomerulus. It is expected that under high or low blood pressure, β_b would be enhanced or attenuated, respectively. As described above, cytoskeletal stability is dictated by the relationship between the F-actin and bundles nullclines, and as illustrated in Fig 2B, different parameters move the stable equilibrium points in different directions. Initially, the healthy podocyte is in steady state in its single equilibrium point (Fig 6A). By decreasing the bundle turnover rate, the system is destabilized and progressive damage and effacement of FPs are observed (Fig 6B and 6C). Here in this complex geometry, the interplay of Eq 1 and Eq 2, through diffusion of G-actin, produce marked spatial heterogeneity in the pattern of bundles. The trivial compensatory mechanism would be to restore the original value of β_b after a certain amount of time Δt_1 (Fig 6D). Most of the FPs that survived up to the time of the correction (Fig 6B) would have reached stability after elapsed time Δt_2 (Fig 6E). A similar result is observed if the compensatory mechanism is applied at a later time (S8 Fig). The permanent effacement of several FPs provides a larger pool of actin to be incorporated by the surviving ones, resulting in stronger bundles. This would correspond to the loss of some FPs and the strengthening of others. The timecourse for the bundles in the FPs highlighted by solid arrows is plotted with corresponding solid lines in Fig 6H. The gray arrowhead identifies the time point used for the 3-D snapshots. These spatially asynchronous and irregular timecourses further substantiate the chaotic tendencies of this system.

A second alternative for a compensatory mechanism is the decrease of α_b , representing decreased bundling coefficient or concentration of crosslinks (Fig 6F). We show that this mechanism can potentially achieve equivalent success as the trivial case of restoring β_b . Once again, the sooner the intervention, the smaller the population of damaged FPs (Fig 6F and 6G), and timecourse of FPs identified by dashed arrows represented in dashed lines in Fig 6H and S8 Fig).

We also explored the impact of increasing the positive feedback, α_f , corresponding to hyperactivating Rac1 or other polymerization signals coming from the slit diaphragm (Fig 6I and 6J). Now, high level of polymerized actin is maintained in each of the surviving FPs; however, there is a new mode of oscillation for bundles (and F-actin) along each FP. The simulations suggest that if applied early enough, this compensatory mechanism may help keep the FP morphology intact (Fig 6J). Similarly to the previous cases, the surviving FPs are able to build

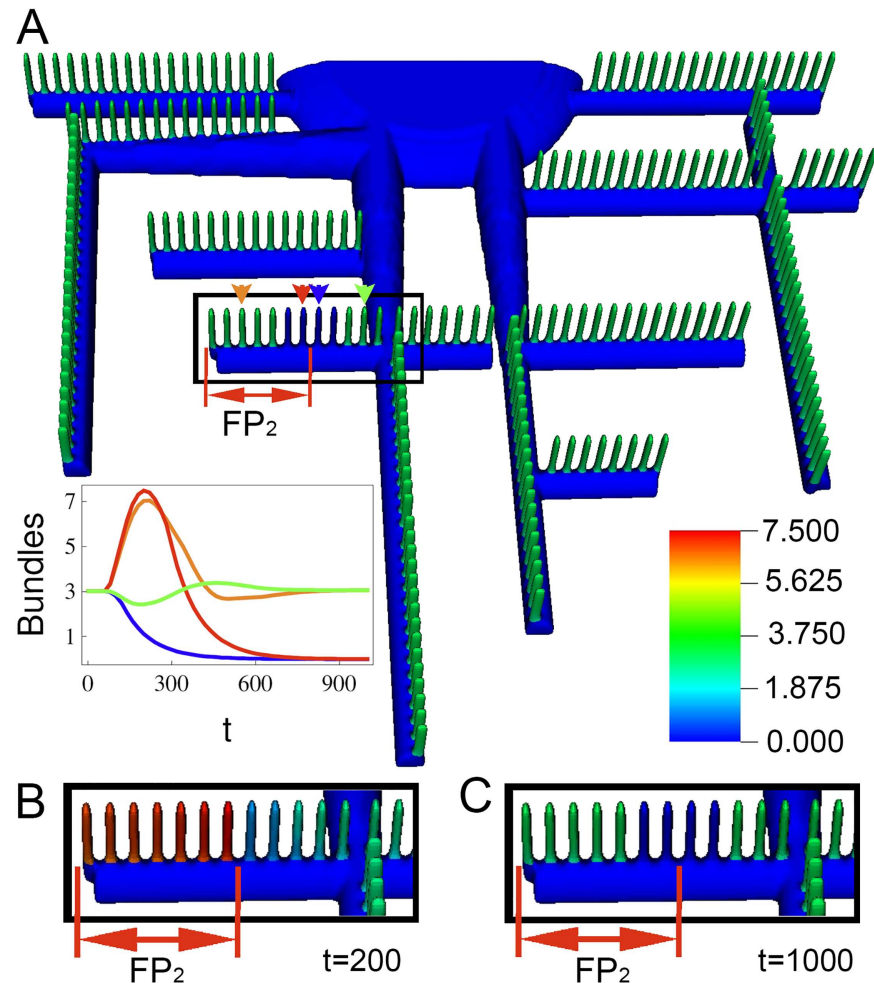


Fig 5. Spatial simulation showing how a transient, localized increase in positive feedback α_f in the region labeled FP_2 impacts actin bundle concentrations in neighboring foot processes. (A) Diagram of a region of a podocyte at steady state. A transient jump in α_f , as in S7 Fig, was locally applied to the region labeled FP_2 and the state of actin throughout the podocyte was simulated over time. The inset shows bundle concentrations over time in four FPs, two within the FP_2 segment and two outside it, identified by colored arrowheads and lines. (B) Zoomed snapshot of the highlighted region is at time = 200 and (C) time = 1000.

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stronger bundles, and in spite of the oscillatory behavior, equivalent number of FPs seem to be preserved in comparison to the previous examples (Fig 6J, 6E and 6G). The overall conclusion is that there are several potential compensatory mechanisms that may be activated to restore FP stability, and the sooner the regulatory response is activated, the larger the number of surviving FPs.

Discussion

We acquired 3-D electron microscope imaging data of rat kidney glomeruli, individually segmented podocytes, and quantitatively analyzed their morphological features to determine the average volume and surface area of the cell body, major processes, and foot processes. This resulted in construction of a representative 3-D podocyte model that is amenable to PDE-based reaction-diffusion modeling with physiologically relevant mechanisms. To the best of our knowledge, this is the first time such a detailed quantitative reconstruction was ever

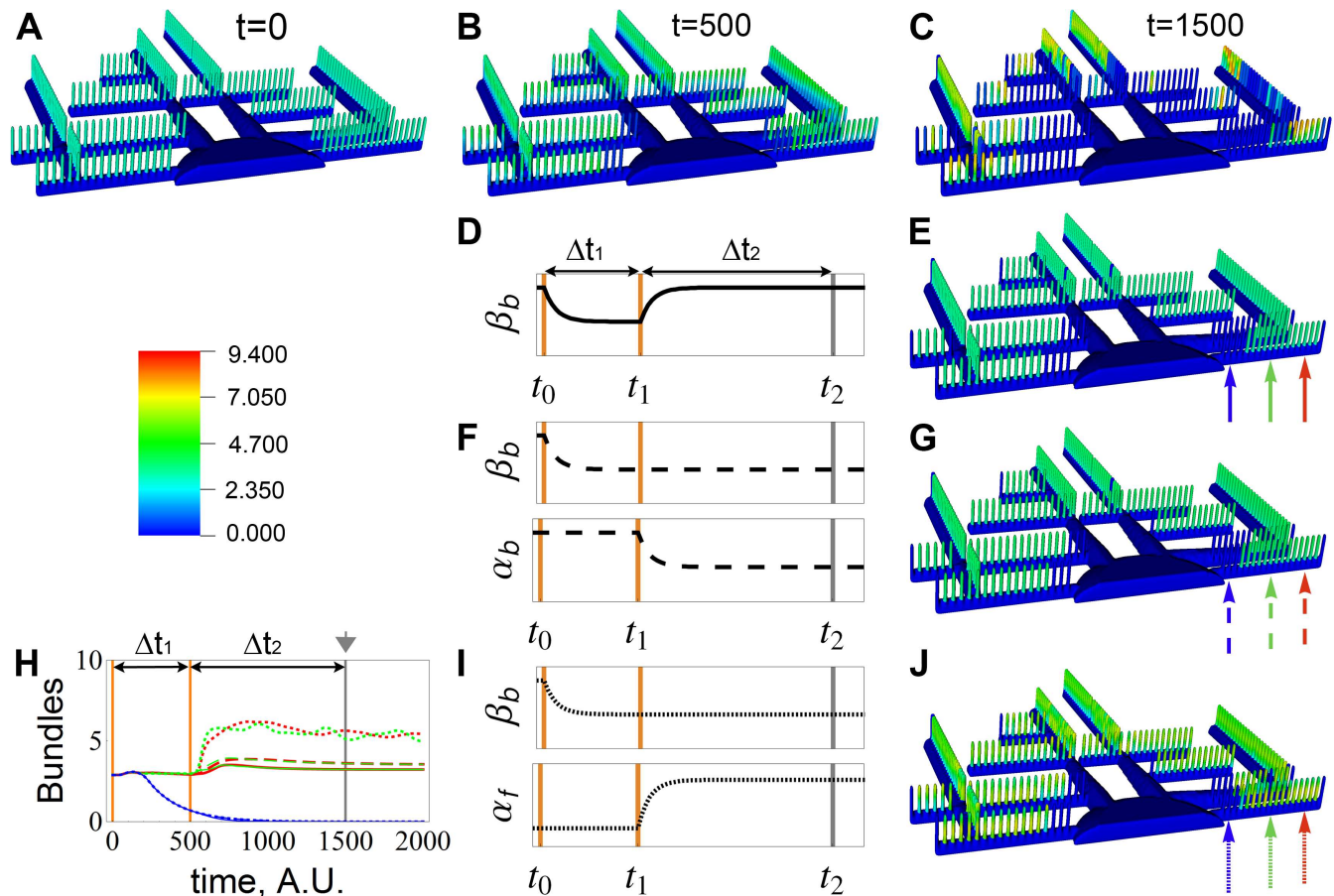


Fig 6. Spatial simulations of the response to perturbed bundling activity, β_b , highlighting potential compensatory mechanisms for actin instability. **A-C.** Progressive loss of FPs due to a continued decrease of β_b imposed at time $t = 0$; snapshots at time **(A)** $t = 0$, **(B)** $t = 500$, and **(C)** $t = 1500$. **D-J.** Tests of combinations of transient perturbation in β_b and α_f to explore compensatory mechanisms. **(D)** Return to baseline β_b at time $t_1 = 500$ results in **(E)** recovery of the majority of the remaining foot process bundle concentrations at $t_2 = 1500$. **(F)** Decrease of α_b at time t_1 while holding β_b constant results in **(G)** similar stabilization. Finally, **(I)** increase of α_f while holding β_b constant **(J)** produces similar spatial results. All three interventions prevent progressive effacement (compare C with E, G and J). **(H)** Timecourses for spatial average of bundle concentration in the FPs identified by arrows in snapshots E, G and J (at time 1500, gray arrowhead). Linestyle follows the same pattern as arrows. The same color scale is used for all the 3-D snapshots of bundle concentrations. Parametric perturbations are listed in S1 Table.

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achieved. The variability in the geometrical parameters measured between the five cells of Table 1 was remarkably small. Through our morphometric analyses, we show that the FPs corresponded to 20% of the volume of the podocyte, while doubling its surface area. Consequently there is a large pool of diffusive monomeric G-actin that is available for the FPs. However, the G-actin pool is not instantly or uniformly available: the monomers must diffuse across the different regions of the cell. Our representative podocyte geometry carefully preserved the length-scales, volumetric and diffusive properties, quantity and distribution of FPs, primary processes, and cell body, thus enabling physiologically relevant simulations. The range of spatiotemporal dynamics within the real geometries of podocytes is likely to be broader than this idealized geometry, but we feel that this idealized geometry will be representative; it also has the advantage of being more computationally tractable, both in simulation time and for analysis of simulation results.

To explore the consequences of the unique podocyte morphology on the maintenance of cytoskeletal integrity of the FPs, we developed a minimal model of actin dynamics and compared non-spatial (ODE-based) simulation results with full reaction-diffusion (PDE-based)

models in the constructed geometry. The minimal model represents key regulatory mechanisms controlling actin polymerization and filament bundling. It contains positive feedback in actin polymerizations, representing Arp2/3-dependent branching nucleation on preformed mother filaments. This positive feedback results in regions of parameter space that produce oscillatory F-actin and bundle kinetics in the ODE simulations (Fig 2). Another mechanism that would be similarly represented by this positive feedback is actin polymerization downstream of nephrin phosphorylation and Nck localization to the FP slit diaphragm. However, it should be emphasized that we did not model the detailed biochemistry regulating actin polymerization and bundling, some of which is still unclear. Rather, our model uses a reasonable level of biochemical specification that allows us to focus on the influence of the complex geometry of the kidney podocyte.

Spatial simulations explicitly consider the process of diffusion of G-actin in and out of FPs from the large reservoir of the cell body and primary processes. The interplay of this diffusion and the positive feedback inherent in the actin dynamics can produce sharp regional differences in the level of actin bundling within closely neighboring FPs. Without bundled actin, the FP would be resorbed into the parent process leading to effacement. Therefore, we assumed that the loss of bundles in FPs leads to loss of structural integrity. Even when a change in bundling activity is distributed uniformly throughout the cell, an apparently chaotic, spatiotemporal pattern of bundle formation and collapse is observed in the FPs (Fig 3). One of the major unanswered questions in podocyte biology is the source of the inherent heterogeneity in podocytopathies. Diseases, such as focal segmental glomerular sclerosis, affect only a subpopulation of podocytes with a large spatial variability in disease etiology. Based on our spatial dynamical model simulations, we suggest that even global changes in stress (e.g., due to hypertension) can lead to selective effacement of FPs with large spatial variability, which may explain the pathophysiological disease progression of numerous podocytopathies.

The balance of Rac1 and RhoA activity (that is represented respectively by actin polymerization and bundling in the model) needs to be tightly regulated to maintain FP stability. This is all the more critical in FPs, where these molecules may be present at low copy number and result in potential stochastic instabilities. Stress (whether focal or global, transient or continuous) can lead to spatially heterogeneous chaotic behavior, and ultimately, to irregular heterogeneous patterns of bundle collapse in FPs. Fig 4 shows how transient activation of Rac1 (i.e., actin polymerization) in one collective region of FPs can shift the steady state balance between F-actin and bundles in all regions. A much more localized transient perturbation, as shown in the spatial simulation of Fig 5, can produce *permanent* changes in the bundle distribution within the system, both within the perturbed region and its immediate vicinity. Unfortunately, experimentally accessible live podocyte models that retain this cell's unique morphology are not yet available. When this experimental problem is solved, direct manipulation of the regulatory mechanisms (e.g. using local photoactivation of RhoA or Rac1 [38]) will help to test whether the chaotic responses predicted by our model can be validated.

Direct damage to FPs, due to high blood pressure for example, can be captured in the bundling turnover parameter β_b . Changing β_b globally, but transiently, can produce permanent changes in bundle distribution (Fig 6A–6C); the severity of FP effacement (represented by loss of bundles) is directly related to the duration of the perturbation. It is possible that regulatory mechanisms could be modulated to alter Rac1 and RhoA activities in response to stress to ameliorate the imbalance. The behavior of the system under three potential compensatory interventions in response to lowered β_b are explored in Fig 6D–6J. These, too, could be tested experimentally once an appropriate *in vivo* or culture preparation is established.

The model for the actin cytoskeleton of the podocyte FP provides a framework for understanding recent findings on the *in vivo* activity levels of the small GTPases RhoA and Rac1.

Our model captures the need for a balance between polymerizing, bundling, and turnover rates for the actin cytoskeleton. Our results are consistent with the observations that a minimum level of RhoA is necessary; however, hyperactivity results in destabilization and progressive loss of FPs [16]. We propose that upon inhibition of Rac1, the cell may sustain its FP integrity with sufficient levels of actin bundles. Signaling through nephrin stimulates actin polymerization, which could also influence the parameter α_f ; similarly, mutations in crosslinking proteins would impact the parameter α_b . Changes in either of these positive feedback parameters for polymerization may give rise to a second equilibrium point for the system, decreasing its robustness.

We hypothesize that healthy cells present a set of parameters that result in a single equilibrium point, representing FPs with strong bundles. In such circumstances, all FPs are stable and have identical properties. Using a reconstructed geometry, we studied the impact of parametric inhomogeneity. Simulations using a representative geometry with features that are important for the diffusion process (such as distances, cross sectional areas and surface area-to-volume ratios for FPs, primary processes and cell body) were used to study the crosstalk between G-actin whole-cell diffusion and the localized polymerization of F-actin in FPs, followed by crosslinking into bundles. As demonstrated here, G-actin availability was a limiting factor, and strong localized polymerization may disrupt the cytoskeleton of FPs elsewhere. The diffusion limited G-actin availability may also disrupt otherwise synchronized oscillations. This results in slow and progressive loss of bundles, the surrogate for effacement of FPs. Of course, the sudden localized collapse of actin structures may be driven by a local inhibitory effect (either decreased polymerization rate constant or enhanced turnover). However, in this work, we demonstrate the feasibility of an alternative hypothesis: enhancing polymerization in remote regions of the podocyte, by a number of signaling pathways, may sufficiently disrupt the balance of G-actin availability to irreversibly drive the local collapse of existing FPs.

Materials and methods

Methods for processing of podocyte images and analysis of podocyte morphology are detailed in *Supporting Material*. The analysis of the ODE model was performed in Mathematica (Wolfram) and the spatial simulations of PDEs in Virtual Cell (VCell.org). The full VCell model is named “Falkenberg:PodocyteStability” and may be accessed through vcell.org. Segmented and reconstructed SBEM imaging data can be obtained through Dryad data repository at doi: 10.5061/dryad.09d0k. Further details of computational methods and analyses are presented in *Supporting Material*.

Supporting information

S1 Fig. (A) Branching patterns with nodes (labeled in boxes) and distances (numbers over arrows) for two different cells. Node ‘1’ corresponds to the center of the cell (core). (B) Histograms for the distances of individual branches of primary and secondary processes for the five adult rat podocytes showed remarkable similarity.

(TIF)

S1 Table. Parameters used in model for each figure, as in Eqs 1–3. The parameter $k = 0.22$. Values differing from the ones used in Fig 2C are in bold. All units are arbitrary.

(PDF)

S2 Table. Nomenclature used in the spatial VCell model.

(PDF)

S2 Fig. Comparison of phase plane diagrams for different values of parameters where ‘n’ represents actin nucleation coefficient and the Hill coefficient ‘h’ represents the positive feedback for F-actin polymerization. While the locations of the equilibrium points are altered, the qualitative relationship between the nullclines is unchanged.
(TIF)

S3 Fig. As in the model of the main text, hyperactive bundling, α_b , (value 0.05 in this figure vs. 0.03 in S2 Fig) will either destabilize the bundles or cause their total collapse.
(TIF)

S4 Fig. Consistent with Fig 2C and 2D, decreasing the parameter α_f from 0.32 (Fig 2C) to 0.1 (Fig 2D) will shift the system from having a single stable point (2C) to having three equilibrium points (two stable and one unstable, 2D). Other parameters as indicated in S1 Table.
(TIF)

S5 Fig. (A) Time course for transient stimulus imposed on the positive feedback α_f for fraction FP_2 or all FPs, and trajectories for concentrations of F-actin and bundles in the foot processes corresponding to regions FP_1 (constant α_f) and FP_2 (transiently stimulated). **(B)** Trajectory for FP_1 . The time point of the peak and end of stimulus are represented in purple and magenta, respectively, in all plots. Time point zero is in black (at identical concentrations for FP_1 and FP_2) and steady-state value for each fraction is represented by shades of blue. **(C)** Steady state bundles in fractions FP_1 (blue) and FP_2 (red) as a function of stimulus intensity. **(D)** Trajectory for FP_2 . The time point of the peak and end of stimulus are represented in purple and magenta, respectively, in all plots. Time point zero is in black (at identical concentrations for FP_1 and FP_2) and steady-state value for each fraction is represented by shades of red. The intensity of the stimulus will alter the relative position between the two trajectories for unstimulated (FP_1) and stimulated (FP_2) fractions. Consequently, for sufficiently large perturbations, either region may collapse.
(TIF)

S6 Fig. Steady state concentrations of bundles in unstimulated (FP_1 , blue) and transiently stimulated (FP_2 , red) fractions of FPs as a function of stimulus intensity. Over a broad range of fractions of FP_1 and FP_2 either region of the cell is subject to damage (collapse of bundles) if the perturbation is sufficiently strong.
(TIF)

S7 Fig. Virtual Cell plot showing time course of the parameter α_f in region FP_2 (purple) and region FP_1 (light brown). The spatial results for bundle concentration are shown in Fig 5. Nomenclature for parameters is described in S2 Table.
(TIF)

S8 Fig. Investigating possible compensatory stimuli against progressive loss of actin bundles within FPs. (A) Initial concentration of bundles at $t = t_0$ where β_b is reduced. The result is heterogeneous loss of bundles in some FPs at times **(B)** $t = t_0 + 500$ and **(C)** $t = t_0 + 1500$. Three lower rows of panels show the three different scenarios under which the bundling could be modified after a finite time, t_1 following injury: **(D)** the parameter β_b recovers its original value and the stabilized FPs can be observed after **(E)** $t_1 = 500$ or **(F)** $t_1 = 1500$. **(G)** Parameter β_b can be decreased to compensate after t_1 and stabilized FPs can be observed at **(H)** $t_1 = 500$ or **(I)** $t_1 = 1500$. **(J)** Alternatively, increase in α_f can also halt loss of bundles in FPs whereby stabilized FPs can be observed at **(K)** $t_1 = 500$ or **(L)** $t_1 = 1500$. We can visualize the timecourses for bundle concentrations in randomly selected FPs (as identified by color-coded arrows) at

(M) $t_1 = 500$ or (N) $t_1 = 1500$. Line style follows the same pattern as arrows, and corresponds to value of a single voxel in the middle of the corresponding FP. All 3-D snapshots follow the same color scale shown in bottom left (except for L, represented with skewed scale in parentheses). Under all of these scenarios, an earlier intervention leads to markedly improved homogeneous restoration of bundles. This can be clearly seen by the difference between the early intervention within the middle column (E, H, K) and late intervention within the right column (F, I, L).

(TIF)

S1 Video. 3-D rendered rotating view of three neighboring rat podocytes.

(MOV)

S2 Video. Time course of FP bundle concentrations after local transient modification of bundling as shown in Fig 5.

(MPG)

S3 Video. Time course of FP bundle concentrations after local transient modification of bundling on a larger region.

(MPG)

S1 Dataset. Nodes and relative branch distances for the five rat kidney podocytes.

(PDF)

S1 Supplementary Materials and Methods.

(PDF)

S1 Text. Description of data deposited to Dryad.

(DOCX)

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Author Contributions

Conceptualization: CVF LML RI EUA.

Data curation: CVF EUA.

Formal analysis: CVF EUA.

Funding acquisition: EUA JChE LML RI MHE.

Investigation: CVF EUA TJD.

Methodology: CVF EUA MHE LML RI.

Project administration: RI LML MHE JChE.

Resources: MS MHE TJD JChO YC.

Supervision: RI LML.

Validation: CVF EUA RI LML.

Visualization: CVF EUA.

Writing – original draft: CVF EUA.

Writing – review & editing: CVF EUA RI LML.

References

- Bertram JF, Messina A, Dillane PC, Ryan GB. Glomerular podocytes in cultured rat kidney slices. A qualitative and quantitative electron-microscopic study. *Cell Tissue Res*. 1989; 256(2):419–29. PMID: [2731225](#)
- Pavenstadt H, Kriz W, Kretzler M. Cell biology of the glomerular podocyte. *Physiological reviews*. 2003; 83(1):253–307. <https://doi.org/10.1152/physrev.00020.2002> PMID: [12506131](#)
- Reiser J, Kriz W, Kretzler M, Mundel P. The glomerular slit diaphragm is a modified adherens junction. *Journal of the American Society of Nephrology: JASN*. 2000; 11(1):1–8. PMID: [10616834](#)
- Kriz W, Hackenthal E, Nobiling R, Sakai T, Elger M, Hahnel B. A role for podocytes to counteract capillary wall distension. *Kidney international*. 1994; 45(2):369–76. PMID: [8164421](#)
- Haraldsson B, Nystrom J, Deen WM. Properties of the glomerular barrier and mechanisms of proteinuria. *Physiological reviews*. 2008; 88(2):451–87. <https://doi.org/10.1152/physrev.00055.2006> PMID: [18391170](#)
- Kriz W, Shirato I, Nagata M, LeHir M, Lemley KV. The podocyte's response to stress: the enigma of foot process effacement. *American journal of physiology Renal physiology*. 2013; 304(4):F333–47. <https://doi.org/10.1152/ajprenal.00478.2012> PMID: [23235479](#)
- Welsh GI, Saleem MA. The podocyte cytoskeleton—key to a functioning glomerulus in health and disease. *Nature reviews Nephrology*. 2012; 8(1):14–21.
- Katsuya K, Yaoita E, Yoshida Y, Yamamoto Y, Yamamoto T. An improved method for primary culture of rat podocytes. *Kidney international*. 2006; 69(11):2101–6. <https://doi.org/10.1038/sj.ki.5000398> PMID: [16625147](#)
- Reiser J, Sever S. Podocyte biology and pathogenesis of kidney disease. *Annu Rev Med*. 2013; 64:357–66. <https://doi.org/10.1146/annurev-med-050311-163340> PMID: [23190150](#)
- Mathieson PW. The podocyte cytoskeleton in health and in disease. *Clin Kidney J*. 2012; 5(6):498–501. <https://doi.org/10.1093/ckj/sfs153> PMID: [26069792](#)
- Saleem MA, Ni L, Witherden I, Tryggvason K, Ruotsalainen V, Mundel P, et al. Co-localization of nephrin, podocin, and the actin cytoskeleton: evidence for a role in podocyte foot process formation. *Am J Pathol*. 2002; 161(4):1459–66. [https://doi.org/10.1016/S0002-9440\(10\)64421-5](https://doi.org/10.1016/S0002-9440(10)64421-5) PMID: [12368218](#)
- Shankland SJ, Pippin JW, Reiser J, Mundel P. Podocytes in culture: past, present, and future. *Kidney Int*. 2007; 72(1):26–36. <https://doi.org/10.1038/sj.ki.5002291> PMID: [17457377](#)
- Huber TB, Benzing T. The slit diaphragm: a signaling platform to regulate podocyte function. *Current opinion in nephrology and hypertension*. 2005; 14(3):211–6. PMID: [15821412](#)
- Saleem MA, O'Hare MJ, Reiser J, Coward RJ, Inward CD, Farren T, et al. A conditionally immortalized human podocyte cell line demonstrating nephrin and podocin expression. *Journal of the American Society of Nephrology: JASN*. 2002; 13(3):630–8. PMID: [11856766](#)
- Hall A. Rho GTPases and the actin cytoskeleton. *Science*. 1998; 279(5350):509–14. PMID: [9438836](#)
- Asanuma K, Yanagida-Asanuma E, Faul C, Tomino Y, Kim K, Mundel P. Synaptopodin orchestrates actin organization and cell motility via regulation of RhoA signalling. *Nat Cell Biol*. 2006; 8(5):485–91. <https://doi.org/10.1038/ncb1400> PMID: [16622418](#)
- Blattner SM, Hodgkin JB, Nishio M, Wylie SA, Saha J, Soofi AA, et al. Divergent functions of the Rho GTPases Rac1 and Cdc42 in podocyte injury. *Kidney international*. 2013; 84(5):920–30. <https://doi.org/10.1038/ki.2013.175> PMID: [23677246](#)
- Yu H, Suleiman H, Kim AH, Miner JH, Dani A, Shaw AS, et al. Rac1 activation in podocytes induces rapid foot process effacement and proteinuria. *Molecular and cellular biology*. 2013; 33(23):4755–64. <https://doi.org/10.1128/MCB.00730-13> PMID: [24061480](#)
- Wang L, Ellis MJ, Gomez JA, Eisner W, Fennell W, Howell DN, et al. Mechanisms of the proteinuria induced by Rho GTPases. *Kidney international*. 2012; 81(11):1075–85. <https://doi.org/10.1038/ki.2011.472> PMID: [22278020](#)

20. Kistler AD, Altintas MM, Reiser J. Podocyte GTPases regulate kidney filter dynamics. *Kidney international*. 2012; 81(11):1053–5. <https://doi.org/10.1038/ki.2012.12> PMID: 22584591
21. Ichimura K, Miyazaki N, Sadayama S, Murata K, Koike M, Nakamura K, et al. Three-dimensional architecture of podocytes revealed by block-face scanning electron microscopy. *Sci Rep*. 2015; 5:8993. <https://doi.org/10.1038/srep08993> PMID: 25759085
22. White FM. *Heat and mass transfer*. Reading, Mass.: Addison-Wesley; 1988. xviii, 718 p. p.
23. Ditlev JA, Vacanti NM, Novak IL, Loew LM. An open model of actin dendritic nucleation. *Biophysical journal*. 2009; 96(9):3529–42. <https://doi.org/10.1016/j.bpj.2009.01.037> PMID: 19413959
24. Pollard TD, Cooper JA. Actin, a central player in cell shape and movement. *Science*. 2009; 326(5957):1208–12. <https://doi.org/10.1126/science.1175862> PMID: 19965462
25. Ditlev JA, Mayer BJ, Loew LM. There is More Than One Way to Model an Elephant. *Experiment-Driven Modeling of the Actin Cytoskeleton*. *Biophys J*. 2013; 104(3):520–32. <https://doi.org/10.1016/j.bpj.2012.12.044> PMID: 23442903
26. Faul C, Asanuma K, Yanagida-Asanuma E, Kim K, Mundel P. Actin up: regulation of podocyte structure and function by components of the actin cytoskeleton. *Trends Cell Biol*. 2007; 17(9):428–37. <https://doi.org/10.1016/j.tcb.2007.06.006> PMID: 17804239
27. Jones N, Blasutig IM, Eremina V, Ruston JM, Bladt F, Li H, et al. Nck adaptor proteins link nephrin to the actin cytoskeleton of kidney podocytes. *Nature*. 2006; 440(7085):818–23. <https://doi.org/10.1038/nature04662> PMID: 16525419
28. Zhu J, Sun N, Aoudjit L, Li H, Kawachi H, Lemay S, et al. Nephrin mediates actin reorganization via phosphoinositide 3-kinase in podocytes. *Kidney international*. 2008; 73(5):556–66. <https://doi.org/10.1038/sj.ki.5002691> PMID: 18033240
29. Holmes WR, Lin B, Levchenko A, Edelstein-Keshet L. Modelling cell polarization driven by synthetic spatially graded Rac activation. *PLoS Comput Biol*. 2012; 8(6):e1002366. <https://doi.org/10.1371/journal.pcbi.1002366> PMID: 22737059
30. Falkenberg CV, Blinov ML, Azeloglu EU, Neves SR, Iyengar R, Loew LM. A Mathematical Model for Nephrin Localization in Podocyte Foot Processes. *Biophysical Journal*. 2012; 102(3):593a–4a.
31. Huang CH, Tang M, Shi C, Iglesias PA, Devreotes PN. An excitable signal integrator couples to an idling cytoskeletal oscillator to drive cell migration. *Nat Cell Biol*. 2013; 15(11):1307–16. <https://doi.org/10.1038/ncb2859> PMID: 24142103
32. Stricker J, Falzone T, Gardel ML. Mechanics of the F-actin cytoskeleton. *J Biomech*. 2010; 43(1):9–14. <https://doi.org/10.1016/j.jbiomech.2009.09.003> PMID: 19913792
33. Ballestrem C, Wehrle-Haller B, Imhof BA. Actin dynamics in living mammalian cells. *Journal of cell science*. 1998; 111 (Pt 12):1649–58.
34. Uchida K, Suzuki K, Iwamoto M, Kawachi H, Ohno M, Horita S, et al. Decreased tyrosine phosphorylation of nephrin in rat and human nephrosis. *Kidney international*. 2008; 73(8):926–32. <https://doi.org/10.1038/ki.2008.19> PMID: 18256598
35. Ichimura K, Kurihara H, Sakai T. Actin filament organization of foot processes in rat podocytes. *J Histochem Cytochem*. 2003; 51(12):1589–600. <https://doi.org/10.1177/002215540305101203> PMID: 14623927
36. Chang F, Lemmon CA, Park D, Romer LH. FAK potentiates Rac1 activation and localization to matrix adhesion sites: a role for betaPIX. *Mol Biol Cell*. 2007; 18(1):253–64. <https://doi.org/10.1091/mbc.E06-03-0207> PMID: 17093062
37. Benzing T. Signaling at the slit diaphragm. *Journal of the American Society of Nephrology: JASN*. 2004; 15(6):1382–91. PMID: 15153549
38. Wu Yi, Frey D, Lungu OI, Jaehrig A, Schlichting I, Kuhlman B, et al. A genetically encoded photoactivatable Rac controls the motility of living cells. *Nature*. 2009; 461(7260):104–8. <https://doi.org/10.1038/nature08241> PMID: 19693014